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REATIONSHIPS BETWEEN MECHANICAL PROPERTIES OF RAW RAT AND CHARACTERISTICS OF CONNECTIVE TISSUE

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SUMMARY

The relationships between mechanical Measured relationships between mechanical purpose of the space with sinusoidal compression, and connective the space collagen content and Noted with sinusoidal compression, and content and solution, characteristics, such as collagen content and solution. have been <sup>value</sup> characteristics, such as collagen content solubility, collagen network organization, have been solutien muscles (Longissimus dorsi, Studied Semitendinosus, Pectoralis bulls, cull cc Pectoralis profundus and Triceps lateralae) from ten animals (young hot provide any information on connective tissue Not provide any information on connective discussion characteristics. But, 66 % of the variations in Compression content can be assessed with a destructive compression content can be assessed with a destructive compression test.  $P_{\text{Ression}}^{\text{pression}}$  test. No relationship between mean found. A Critical and collagen solubility could be found. A Critical  $c_{ritiCal}^{\text{weeters}}$  and collagen solubility could be found.  $k_{e_{i}}^{\text{best}}$  value of the compression ratio (K = 0.3-0.4)  $v_{leg}^{\rm blean}$  value of the compression ratio ( $\kappa = 0...$  of a  $v_{leg}^{\rm blean}$  defined; it corresponds to the start of a  $v_{legnific}^{\rm blean}$  content and Deen defined ; it corresponds to the source Regificant correlation between collagen content at the characterize collagen f strength. To characterize collagen fibre tension, the connective network has to be put under hension, first. On this basis, the suitability of a characteristic mechanical test to evaluate collagen characteristics has been discussed. MATERIALS AND METHODS

## Muscle sampling

Superiments have been carried out on 4 muscles : Maissing (ID) Semitendinosus (ST), attoralis profundus (PP) and Triceps brachii caput Were

Friesian cull cows and four young Friesian bulls The Used in these experiments. After slaughter, Concesses were conditionned at 15°C for 6 h and then the second state of the second s cooled skilled at 2°C for 2 days. Selected muscles were at 2°C days post-mortem, vacuum packed and stored by 2°C, All at 2°C. All measurements were carried out 8 days post-tortem all measurements were carried out 8 days postpendicularly to the myofibres.

### Analysis Linear

Measured on an enlarged photograph of the slice. The din axis so the slice defined as the largest main dimension, axis of the slice, defined as the largest rossing, was determined. The total number of strongs between this axis and the main perimysium between this (Duront, 1983). The number of <sup>105</sup>Bings between this axis and the main perimysium hetwork was calculated (Dumont, 1983). The number of <sup>Cossings</sup> per length unit along this main axis was <sup>Childered</sup> to the linear density (LD1). Considered to be the linear density (LD1).

Wildered to be the linear density (LD1). Wide content was estimated, after perchloric acid (V.5), by the amount of total hydroxyproline and Loxley (1992) Untrolysis was performed by heating Loxley (1963). Hydrolysis was performed by heating or Much 10020 for 4 h. in 15 ml of 70% Perchloric acid. of muscle at 100°C for 4 h,

Collagen Solubility was determined after heating 3 g Minced muscle at 90°C for 4 h in the following er: The second for the following the second for the following the second for th burger: Tris HCl 0.02 M, pH 7.4. After filtration, the Ween: Tris HCl 0.02 M, pH 7.4. After filtration, and the samples were hydrolysed and hagen under the same conditions. All agen was determined, under the same conditions. the following expression: Solubility percentage was calculated according to

\*ouwing expression:
\*olubility(%)=Total collagen - insoluble collagen
Total collagen

Sarcomere length was determined by diffraction of a loss been been been to the method of Cross et al.  $1_{980}$  beam according to the method of Cross et al.

### Mechanical measurements

The mechanical measurements were carried out with the Food Texture Analysis System (F.T.A.S.) set up by Salé et al. (1984). Meat samples (3 cm x 1 cm x 1 cm) were compressed by a 1cm2 probe perpendicularly to the myofibres in a cell equipped with 2 lateral walls. In these conditions the free deformation of the samples was limited to only one direction, either perpendicular (transversal configuration) or parallel (longitudinal configuration) to the myofibres (fig. 1). The compression ratio varied within a large range,  $0.2 \leq K \leq 0.8$ .

From the stress-strain curves obtained during one sinusoidal compression cycle (period: 0.1s), the following parameters were determined:

▼m (N/cm2) : maximum stress reached during the compression

rt : elasticity factor which was the ratio of the energy almost instantaneously released by the sample during the upward movement of the probe, over the total energy given to it during compression.



Figure 1 - Schématic design of the compression cell with a meat sample in the longitudinal (L) and transversal (T) configurations

#### RESULTS

The characteristics of connective tissue and the sarcomere lengths of the different muscles are indicated in table 1. Large variations in collagen content (5.8-11.6 mg/g fresh tissue), solubility (30.3-36.3 %), linear density (1.85-2.90  $\text{cm}^{-1}$ ) and sarcomere length  $(2.0-2.7\mu)$  were observed. due to muscle factor. Animal influence was reflected in the standard deviations that accounted for 22 %, 36 %,25 % and 20 % of the respective mean values. The LD muscle had the lowest collagen content and linear density, but the highest solubility whilst the ST muscle had the lowest solubility. The PP muscle had the highest sarcomere length and linear density.

Mean Table 1. values of connective tissue characteristics (collagen content COL, solubility SOL, linear density (LD1) and sarcomere length (SL) for different muscles.Standard deviations in brackets.

1.47 6.00	LD	ST	PP	TB	
COL	5.8	10.8	11.3	11.6	
(mg/g)	(0.5)	(1.2)	(2.1)	(2.5)	
SOL (%)	36.3	30.3	31.3	34.9	
	(8.7)	(7.7)	(11.3)	(9.6)	
LD1	1.85	2.48	2.90	2.60	
(cm <sup>-1</sup>	(0.30)	(0.60)	(0.45)	(0.50)	
SL $(\mu)$	2.00 (0.4)	2.06	2.7 (0.3)	2.2	

Table 2. Mean values of maximum stresses (N/cm2) and elasticity factor (%) for different muscles, at 2 compression ratios (K= 0.2 and K= 0.8) and in the longitudinal (L) and transversal (T) configuration (standard deviations in brackets)

Compression	Configuration	LD		ST		PP		TB	
ratio	a to restance	σm	rt	Um	rt	σm	rt	νm	rt
0.2	L	9.8 (2.7)	24.5 · (4.1)	9.5 (2.5)	23.2 (5.3)	17.3 (6.6)	30.5 (7.7)	15.0 (4.0)	23.2 (3.8
	Т	6.9 (2.9)	44.5 (4.7)	7.3 (4.5)	40.8 (10.0)	4.4 (1.5)	33.8 (7.2)	8.0 (3.0)	46.8
0.8	L	47.1 (15.0)	15.0 (2.4)	108.0 (22.0)	20.9 (1.8)	96.6 (18.0)	19.3 (2.4)	84.0 (27.0)	18.2 (2.9
	Т	42.5 (11.0)	15.1 (2.9)	71.0 (9.2)	14.7 (3.5)	83.0 (24.0)	21.5 (3.5)	87.0 (26.0)	18.4

Large standard deviations were also observed for the maximum stresses obtained in various conditions table 2. At a 0.2 compression ratio, the differences between muscles in the longitudinal configuration may be due not only to variations in ageing rates (Lepetit et al., 1986a), but also to differences in sarcomere Since the PP muscle has a larger sarcomere lengths. length, it displayed maximum stress that was higher in the longitudinal configuration, and lower in the transversal configuration. This has been explained (Lepetit et al., 1986b) by the fact that the stretching state of connective tissue network is a function of sarcomere length. The elasticity factor was much higher in the transversal than in the longitudinal configuration, because the myofibre viscous component was not displayed when the free lateral strain was perpendicular to the myofibre axis (Lepetit and Culioli, 1985). Sarcomere length may also have an influence on the rt values, as the PP muscle was more elastic than the other muscles longitudinal configuration, and less elastic in in transversal configuration. At a 0.8 compression ratio, the lowest maximum stresses were obtained with the LD muscles (  $\sim 45 \rm N/cm2)$  , whilst ST, PP and TB muscles had displayed small differences (83 N/cm2  $\leqslant$   $\mathrm{Mm} \leqslant$  108 N/cm2). The gap between transversal and longitudinal values would depend on the muscle. Because of destructive conditions, the elasticity factor was lower than previously and was not influenced by configuration or muscle.

In the non-destructive test (K=0.2). the correlation coefficients between the mechanical parameters (maximum stress and elasticity) determined on raw meat and the collagen content, the solubility or the linear density of connective tissue were fairly low (r  $\leqslant 0.37)$ and in most cases non-significant (table 3).

Table 3. Correlation coefficients (r) between the connective tissue characteristics (collagen content COL, solubility SOL, linear density LD1) and the various mechanical parameters determined at 2 compression ratios (K=0.2, K=0.8) in longitudinal (L) and transversal (T) configurations.

1	f m			K = 0.8				
	σm		rt		𝕶 m		rt	
L	Т	L	Т	L	Т	L	Т	
.31	-0.17	-0.01	-0.09	0.71	0.82	0.58	0.49	
.29	0.05	0.37	0.24	-0.17	-0.14	-0.27	0.03	
.18	-0.11	0.46	-0.05	0.49	0.38	0.38	0.26	
	.31 .29 .18	.31 -0.17 .29 0.05 .18 -0.11 es greater	.31 -0.17 -0.01 .29 0.05 0.37 .18 -0.11 0.46	.31 -0.17 -0.01 -0.09 .29 0.05 0.37 0.24 .18 -0.11 0.46 -0.05	.31 -0.17 -0.01 -0.09 0.71 .29 0.05 0.37 0.24 -0.17 .18 -0.11 0.46 -0.05 0.49	.31 -0.17 -0.01 -0.09 0.71 0.82 .29 0.05 0.37 0.24 -0.17 -0.14 .18 -0.11 0.46 -0.05 0.49 0.38	.31 -0.17 -0.01 -0.09 0.71 0.82 0.58 .29 0.05 0.37 0.24 -0.17 -0.14 -0.27 .18 -0.11 0.46 -0.05 0.49 0.38 0.38	

level

Still, there was a better correlation between collage content and mechanical parameters when the test variations in collage destructive (K=0.8). Thus, variations in colla content explained 67 % (r=0.82) of the variations mechanical resistance measured in the transverse configuration (fig. 2). The relationship between not as collagen content and elasticity was, however,

The correlation coefficient between the linear density of the primary perimysium network and collagen content was nearly 0.5. Yet, the information on college content given by mechanical measurements was improved when linear density was taken into consideration in a multiple regression. This probably due to the fact that LD1 and maximum stress were not independent variables (table 3) and that only the perimysial network was taken into account and not all the perimisual as in the studies all the perimisyal network, Dumont (1983).

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Figure 2 - Variations in maximum stress with collagen content, at 2 compression ratio + K = 0.2; \* K = 0.8, and in transversal configuration

When the compression ratio increased, the correlation between collagen content and maximum stress increase following a signation following a signoidal curve with a point of  $inflex_{i0}^{re}$  at around K=0.4 (fig. 2) at around K=0.4 (fig. 3). The configuration did influence either the shape of the curve noticeably the correlation coefficient values. Collagen solubility, which is an important component of cooked meat tenderness, did not correlate very with the different mechanical parameters determined raw meat (r < 0.37).



Figure 3 - Influence of compression ratio on the correlation coefficient between maximum Street stress and collagen content transversal, o longitudinal configurations

# DISCUSSION - CONCLUSION

Although Compression tests performed on raw meat at stress ( 20 %) allows a good evaluation Nocibrillar properties (Lepetit et al., 1986), did not did hot provide any information on connective tissue that provide any information on connective tissue characteristics, or collagen content and solubility, on network linear density. But destructive compression good estimate of the On network linear density. But destructive intramuscular collagen contents. However collagen ubility intramuscular collagen contents. Solubility cannot be evaluated. These results confirm those of the solution of hose of Kopp and Bonnet (1982) who obtained good Correlations between collagen content and maximum Collagen force measured on raw meat, whatever the collagen solubility.

 $t_{10w.COmpression ratios} (\measuredangle 20\%)$ , the meshes in the compression ratios (  $\measuredangle 20\%$ ), the wavy collagen  $c_{0,m}^{AOW. COMpression ratios}$  ( $\leq 20$  %), the meshes large the competitive tissue are deformed, but the wavy collagen to characterize the tissue are deformed. To characterize the Herective tissue are deformed, but the wavy clare the stars are not directly strained. To characterize the stars the network has to undergo heistance of these fibres, the network has to undergo <sup>Alstance</sup> of these fibres, the network has to uncompression first. This can be achieved only when <sup>appression</sup> is around 30 %, which does not induce any <sup>apprent</sup>. So, a non-destructive Apparent breaking in samples. So, a non-destructive sechanical test should be used in this range of Sechanical test should be used in Connection with myofibre orientation and deformation characterization.

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